



# Microfluidics *and Engineering* *a New Doctor-Patient Interface*

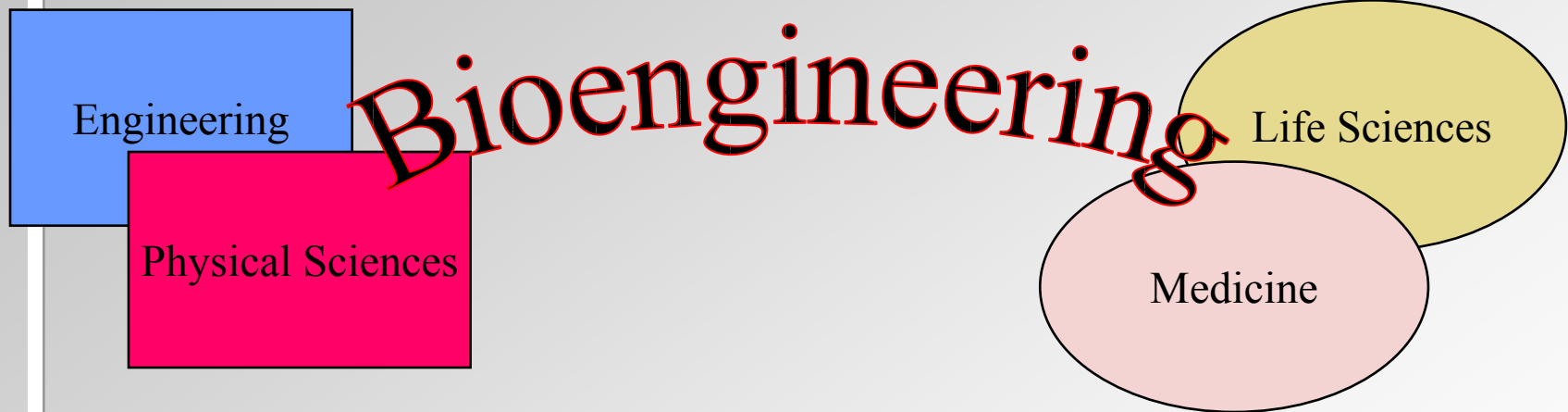
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# A view from the bridge



- Bioengineering is the discipline that will be able to exploit the discoveries of the life sciences and create the technology needed to apply them to the practice of medicine.

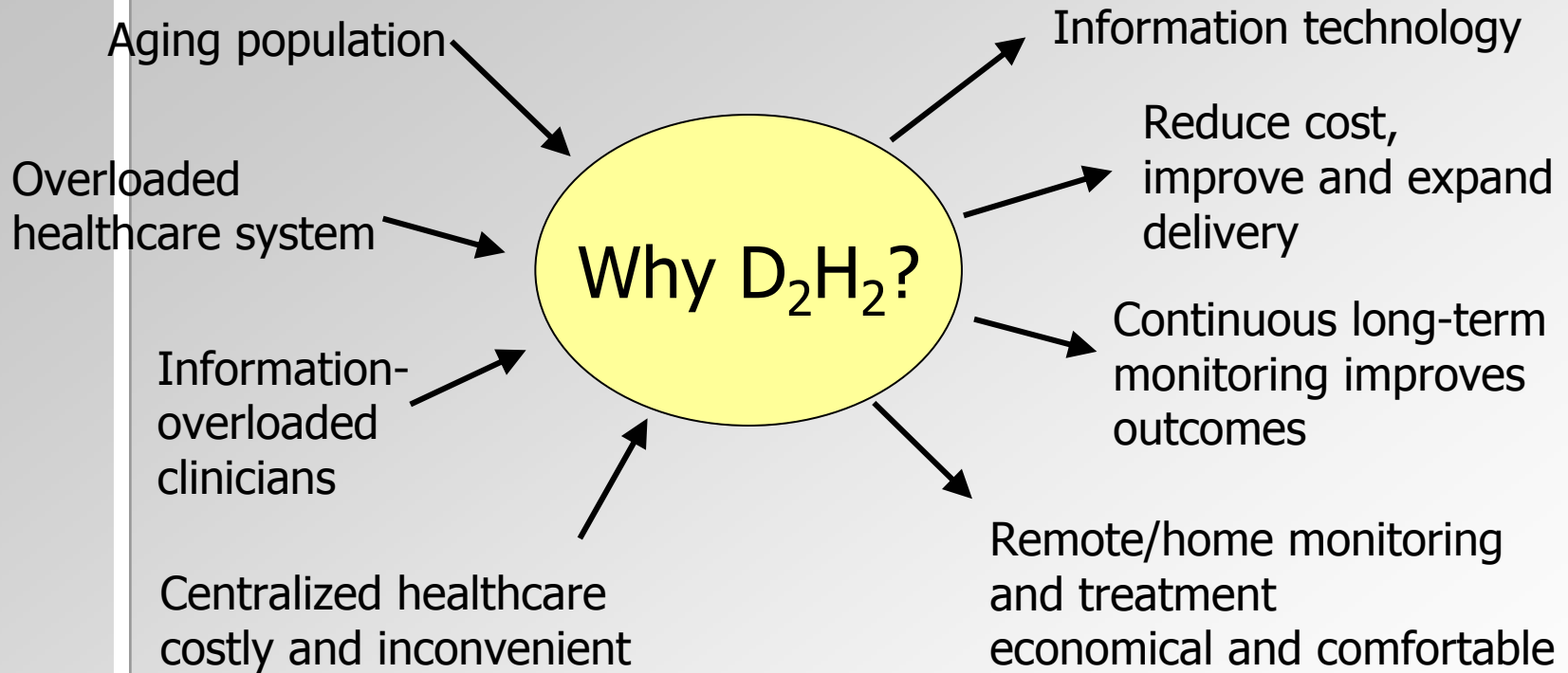


# Bioengineering in transition

- 20th century bioengineers famous for developing excellent medical technology
  - Centralized
  - Expensive to buy, use and maintain
- 21st century bioengineers must look first to
  - Integration into the entire healthcare system
  - Minimizing the cost of the system



# Distributed Diagnosis and Home Healthcare ( $D_2H_2$ )



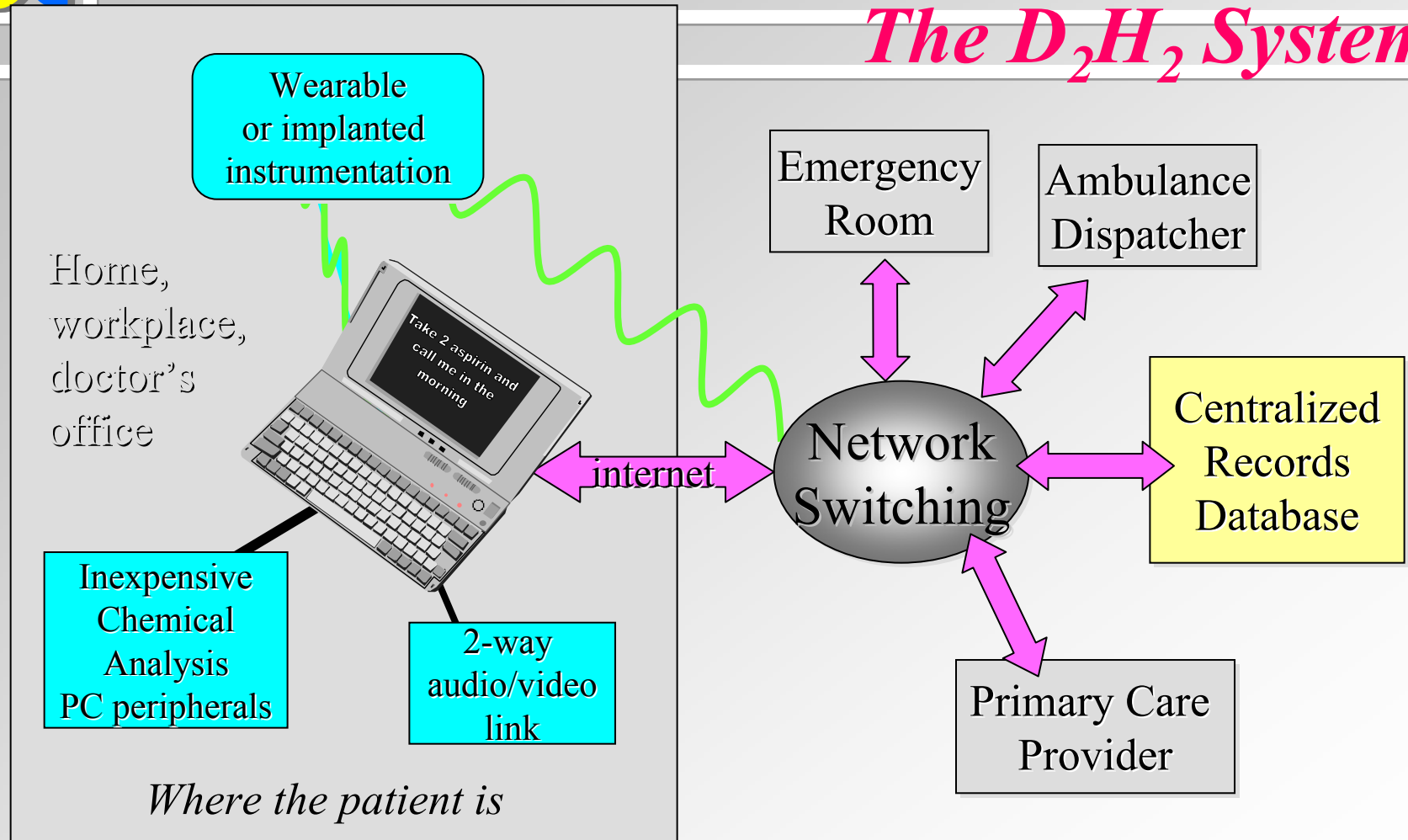
*pushing*

*pulling*



# A New Doctor-Patient Interface

## *The D<sub>2</sub>H<sub>2</sub> System*



*today the hospital, tomorrow the home*



# The Uses of $D_2H_2$

- Hospital inpatients (underway)
- Clinical trials of new medications
- Hospital outpatients (cancer, post-surgery)
- Chronic conditions (cancer, arthritis, AIDS, diabetes, heart disease)
- Monitoring chronic or critical drug treatment
- Pregnant women
- Early warning for emergent health conditions (e.g. heart attack, stroke, heat stress, infection, food poisoning, etc.)



# The Appeal of Microfluidics

- Potential to automate very complex procedures
- Compatibility with small sample volumes
- Potential for packing many devices in small spaces--parallel processing
- Little waste
- Possible integration with pumping, detection and processing components
- Reproducibility of function
- Potential for mass fabrication
- *Potentially* low inherent cost



# Yager Lab Medical Diagnostic Goals

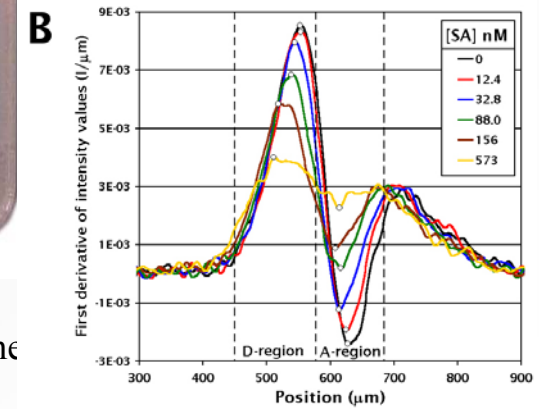
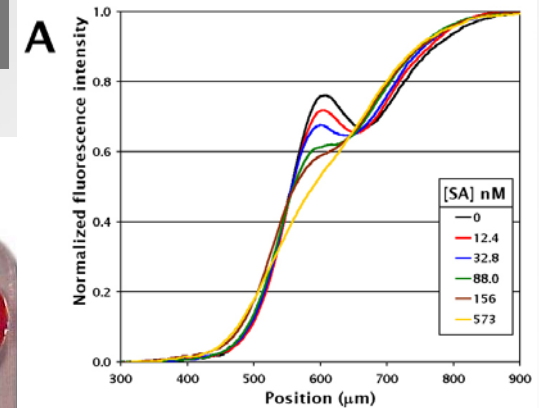
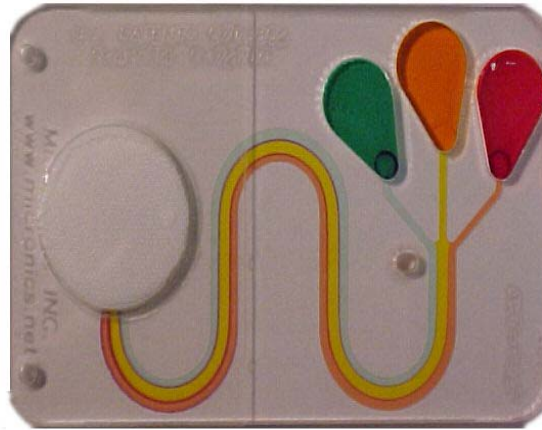
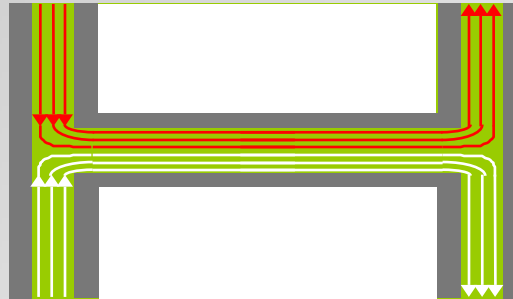
- A disposable polymeric laminate cartridge that:
  - costs less than \$5
  - holds all the chemistry needed for multiple complex quantitative bioassays on a drop or two of biological fluid (*not just blood!*)
  - can be left in the glove compartment of a car all summer in Texas or winter in Alaska
  - requires only insertion in a handheld device to work
  - gives all results in under 5 minutes
  - provides laboratory-quality quantification of analytes
- A portable inexpensive measurement system that supports the use of laminate cartridges

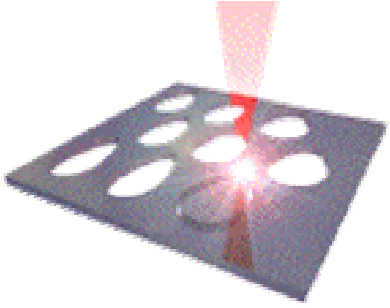




# Technologies Developed Since 1994 at UW or Micronics

- Microfluidic methods and devices:
- H-filter
- T-sensor
- Electrokinetic Fractionation
- Electrokinetic concentration
- Mixers
- Valves
- Switches
- Flow cytometers
- Immunoassays





# WTC/Micronics Rapid Microfluidic Prototyping

QuickTime™ and a  
Animation decompressor  
are needed to see this picture.

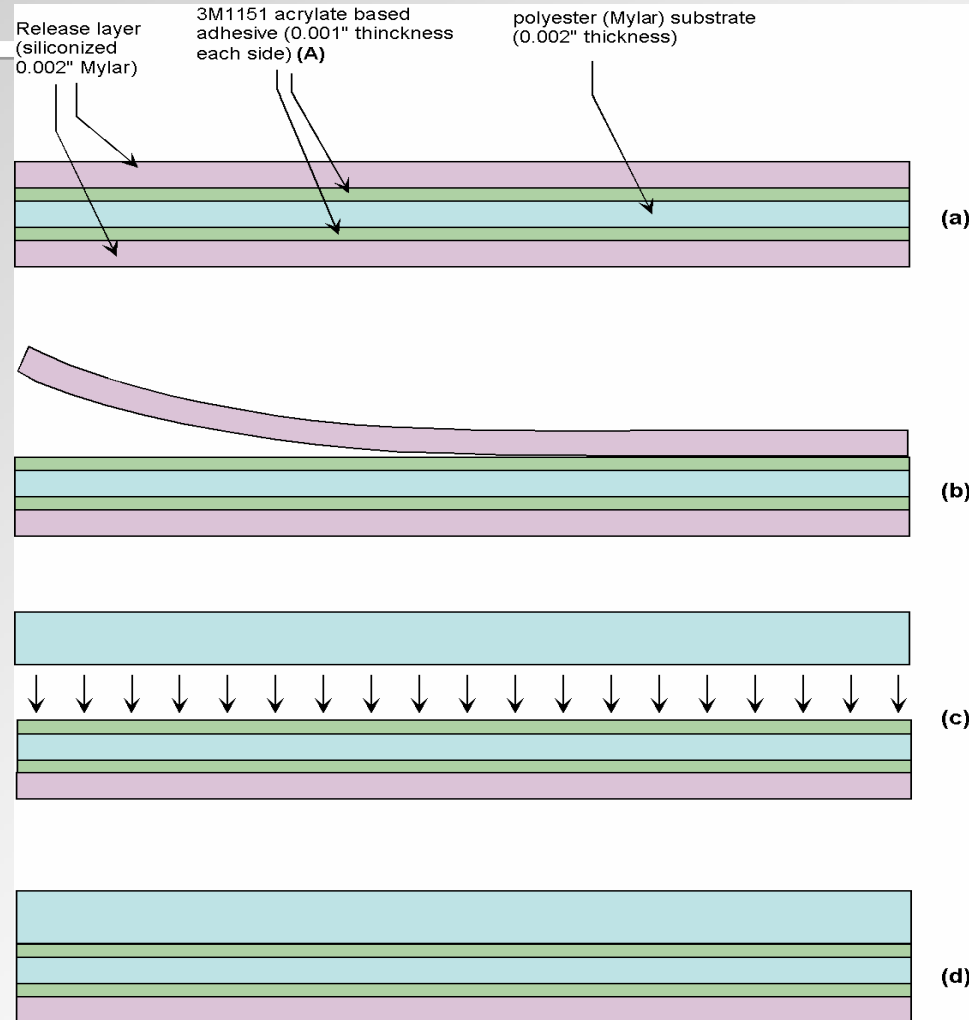


- This CO<sub>2</sub> laser cutting system allows conversion from CAD file to assembled multi-level polymeric laminate **in ~4 hours.**
- This is a powerful new tool for rapid prototyping.
- Assembled laminates compatible with aqueous solvents.



# Lamination

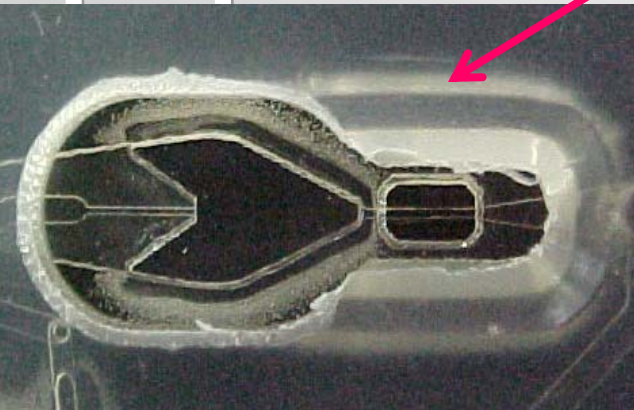
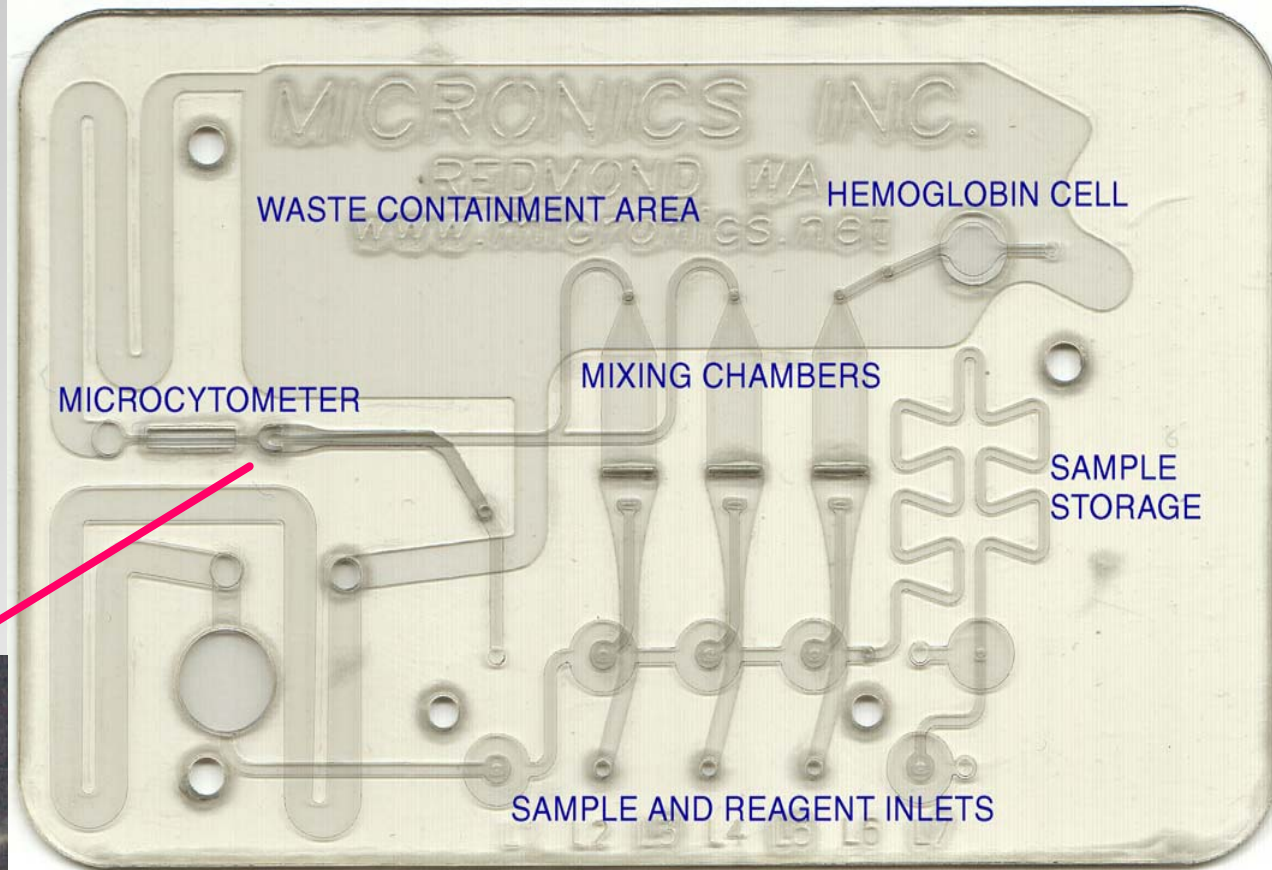
- 0.004" thick Mylar coated on one, both or neither side with 3M1151 Adhesive
- The release layers are removed and subsequent layers are stacked to form desired device geometry





# Integrated Chemical and Cellular Analysis in a Single Disposable

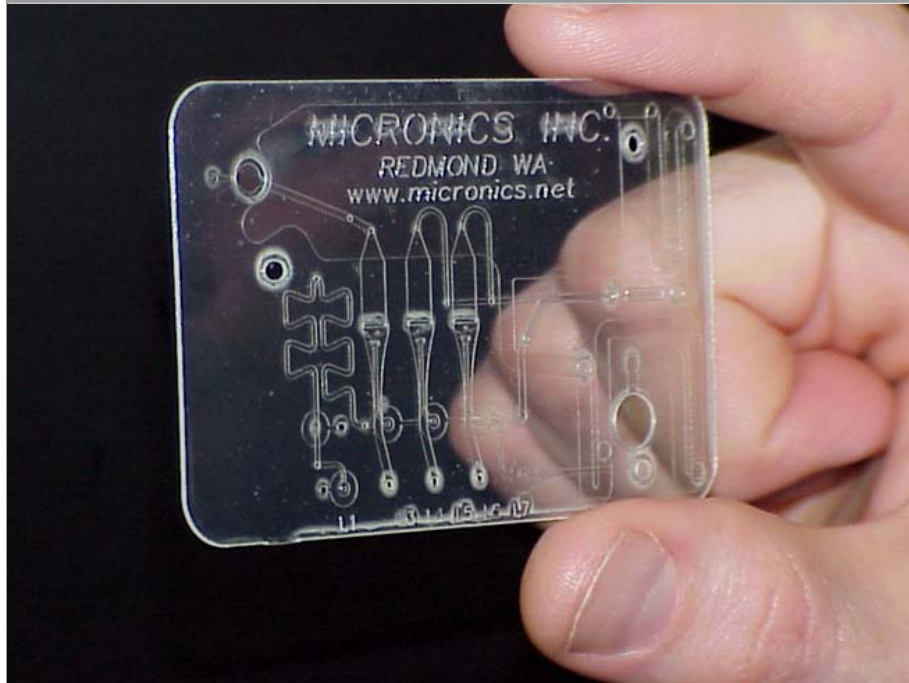
Micronics' 7-layer Mylar laminate hematology cartridge--  
*rapid prototyping and mass fabricability*



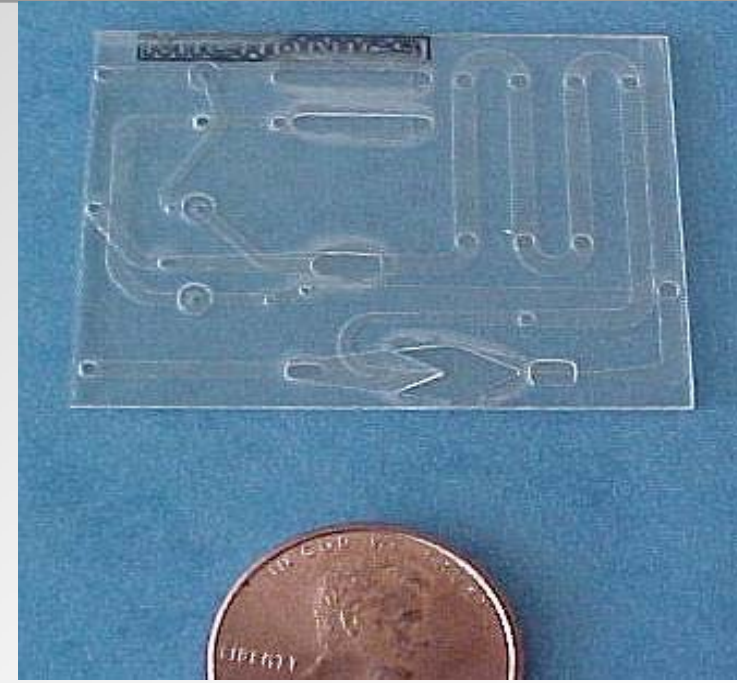




# This technology is *just small enough*



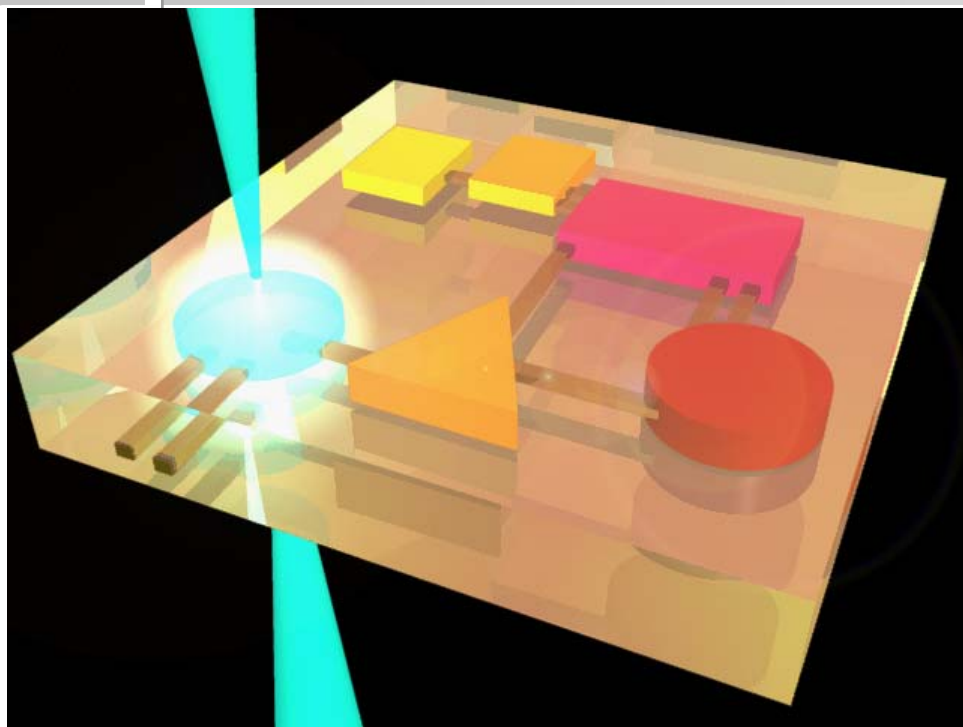
- Micronics demonstrates complete fluidics for a flow cytometry system on a 7-layer microfluidic card



- Under development with Micronics and Honeywell for DARPA is a complete cytometer to fit in a wristwatch.



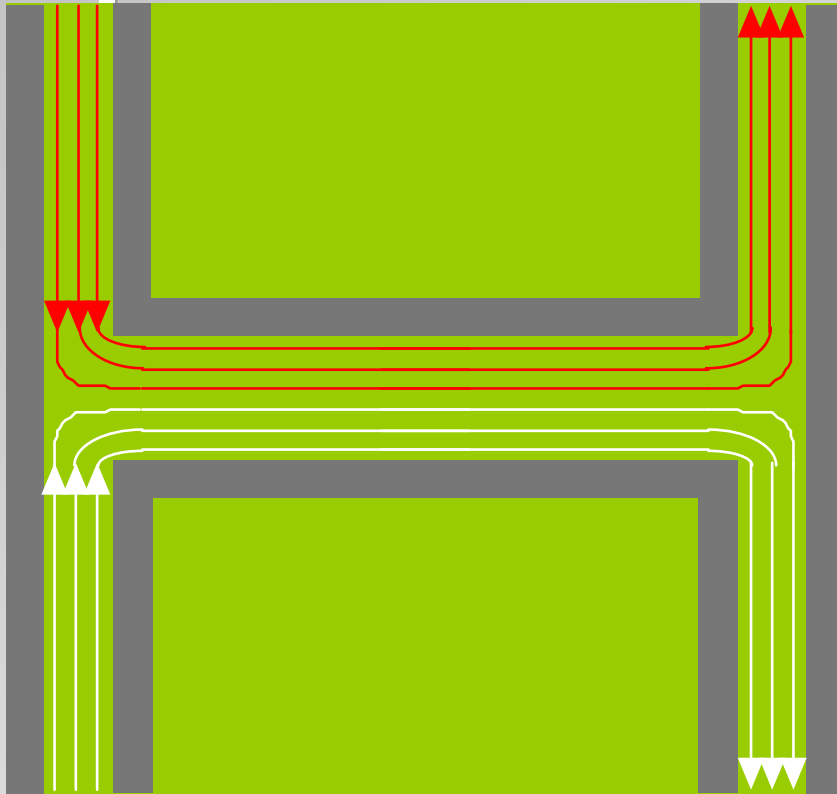
# A “New” Paradigm? Laminate-Based Chemistry



The design of microfluidic systems (be they analytical or synthetic) is *completely analogous* to current design of chemical plants scaled in acres.

- Experiments are designed to be optimal for the small samples used, including multiple processing steps carried out entirely within the laminate.
- Optical and electrical access for real-time analysis by standardized off-laminate instruments are provided.
- If the experiment is not optimal, *redesign and retesting in one day* is straightforward.
- Because the laminates themselves cost only a few dollars, if the experiment works well, the device can be duplicated inexpensively for use at home *and shipped as a file for use by collaborators elsewhere the next day.*

# Develop an H-filter-based microfluidic device capable of extracting a wide range of analytes from the mucins in saliva



- In a thin channel at low Reynolds number, *turbulence cannot exist*.
- Flow streams can run next to each other without mixing; the reversible apposition of two fluids as at left is possible only in devices with small dimensions.
- Diffusion is the dominant transport mechanism between adjacent flow streams.
- Large particles diffuse slowly and stay on their side of the channel; small molecules rapidly diffuse across.
- ***We will extract analytes from the mucins in a flowing stream of saliva with this principle.***



# The DIA: A New Bioassay based on Microfluidics

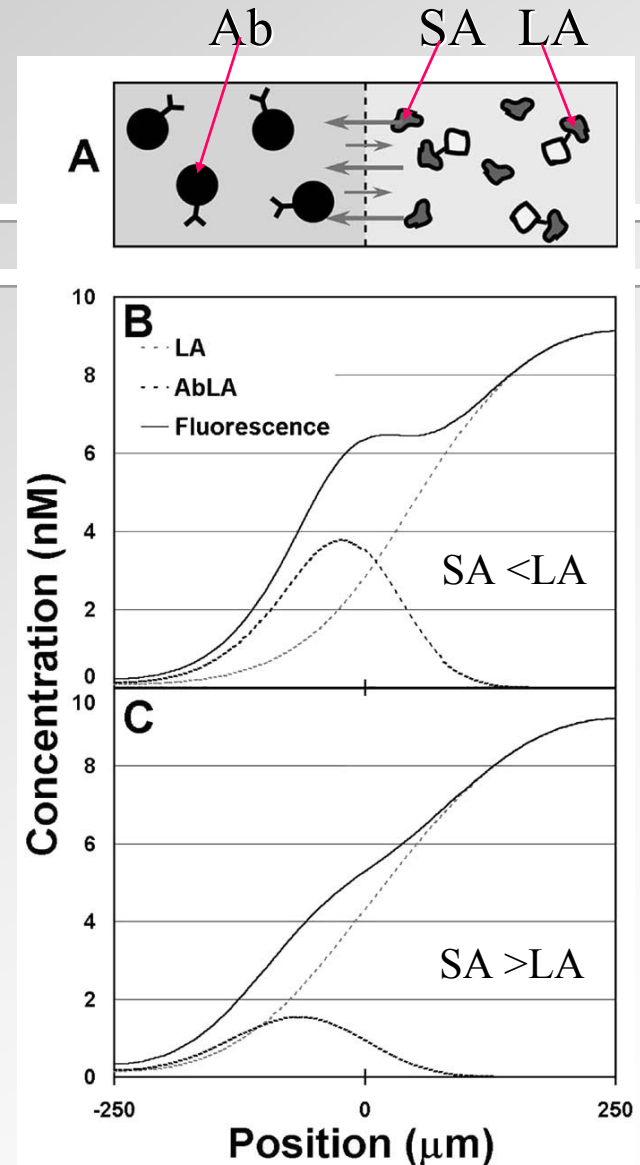
- The T-sensor was shown early on to measure flowing analytes
- Given that immunoassays are central to diagnostics
- Attempt to see if a competition immunoassay could be implemented in a T-sensor
- The Diffusion ImmunoAssay (DIA) based on differential diffusion of small and large molecules





# The DIA: A diffusion-based competition immunoassay

- In the assay the sample antigen (SA) is forced to compete for the antibody (Ab) binding sites with a known quantity of antigen to which a small fluorescent label has been covalently attached (LA).
- If  $[SA]$  is high enough, all of the Ab binding sites are blocked and the LA diffuses as if the Ab were not there!

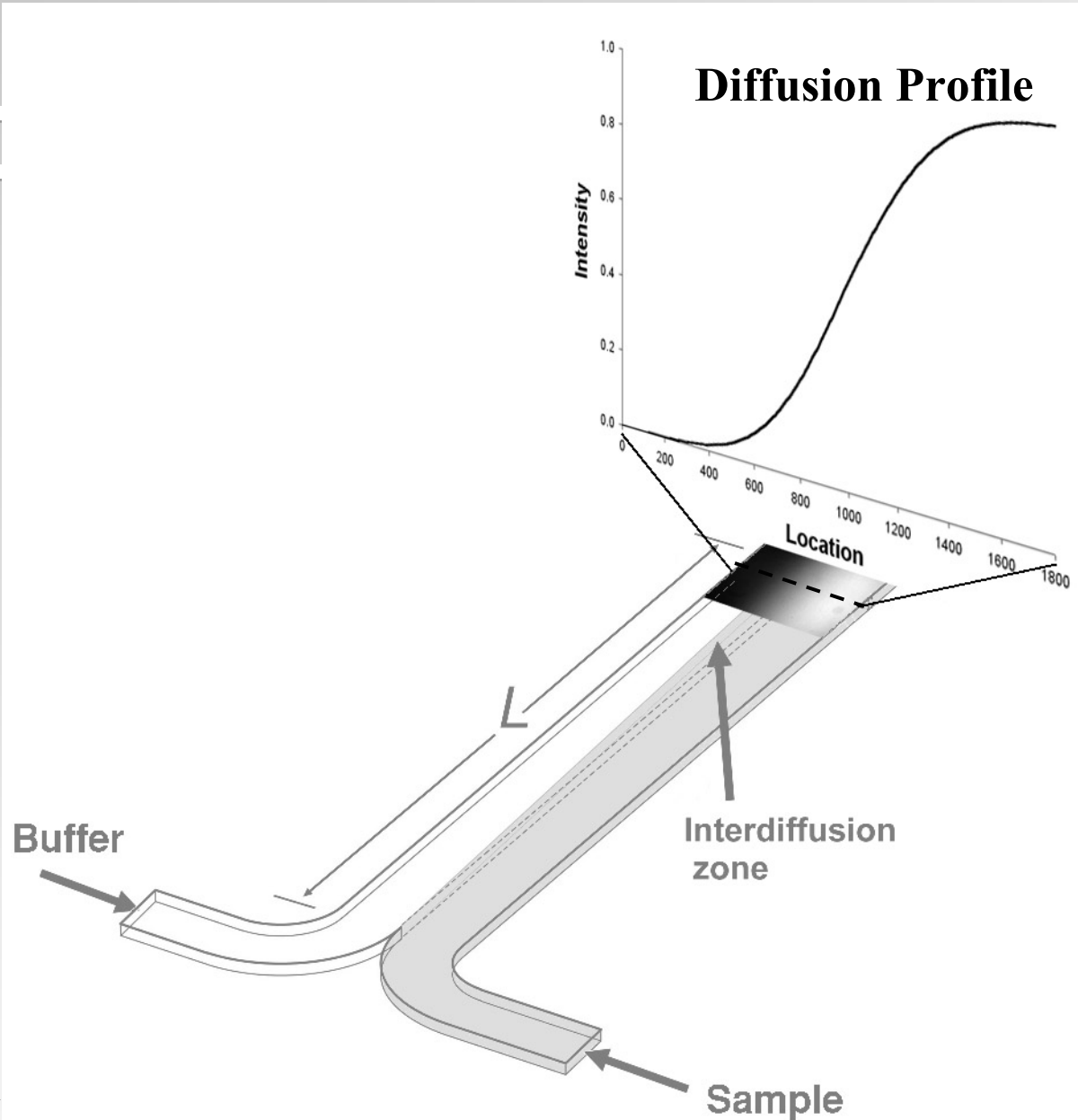




# Measurement with the T-Sensor

Optical imaging along the  $y$  axis (transmission or reflection) allows measurement of concentrations of analytes along  $d$  at a known distance  $L$  downstream (and a known time since contact between solutions).

Interactions between diffusing species and be measured by intensity and position.

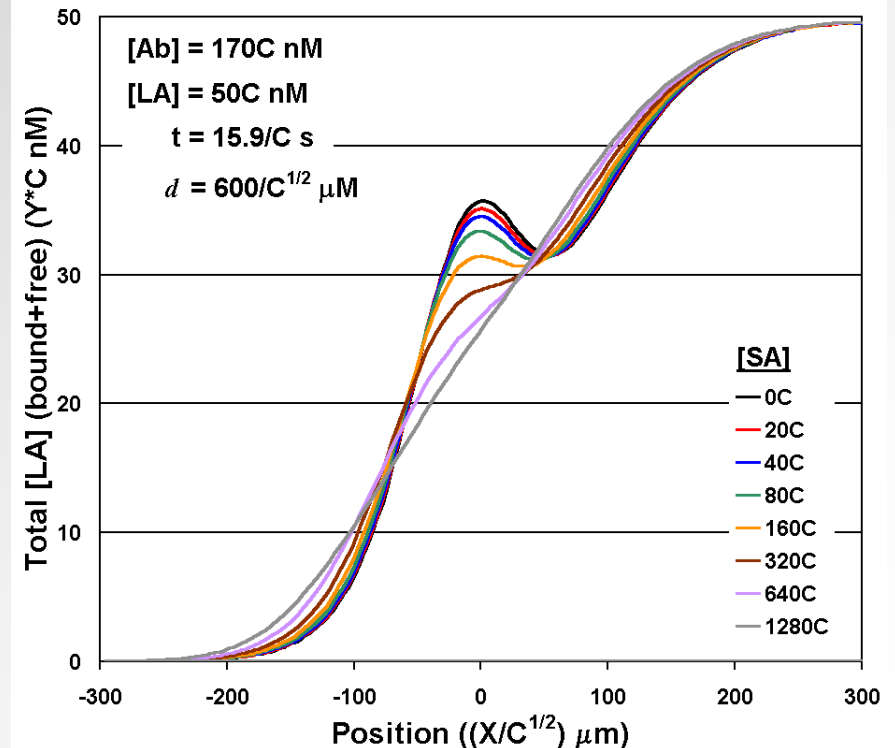
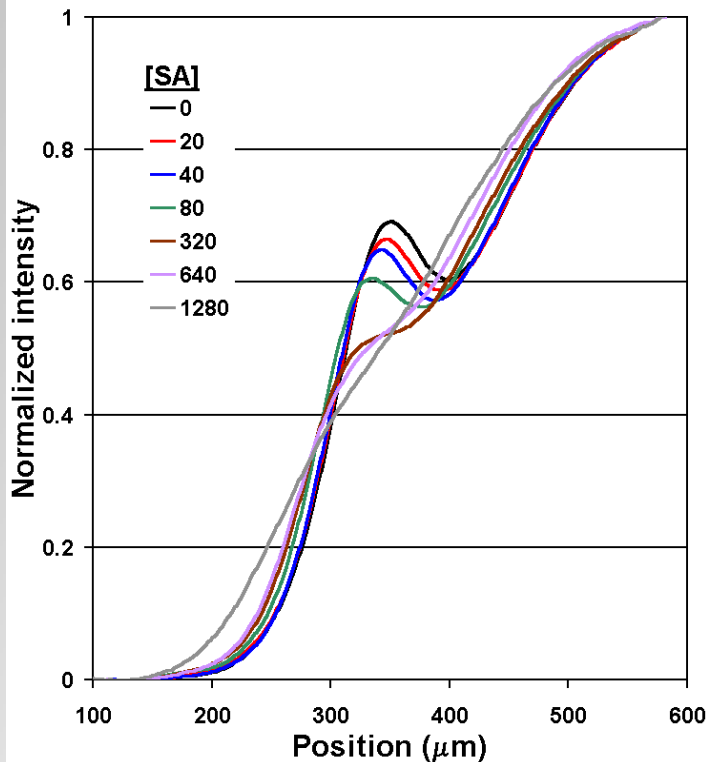




# DIA for Anti-epileptic Drug Phenytoin

- **Experiment:** fluorescence intensities across the T-sensor for [SA] from 0 to 1,280 nM (1000 x lower than in blood)

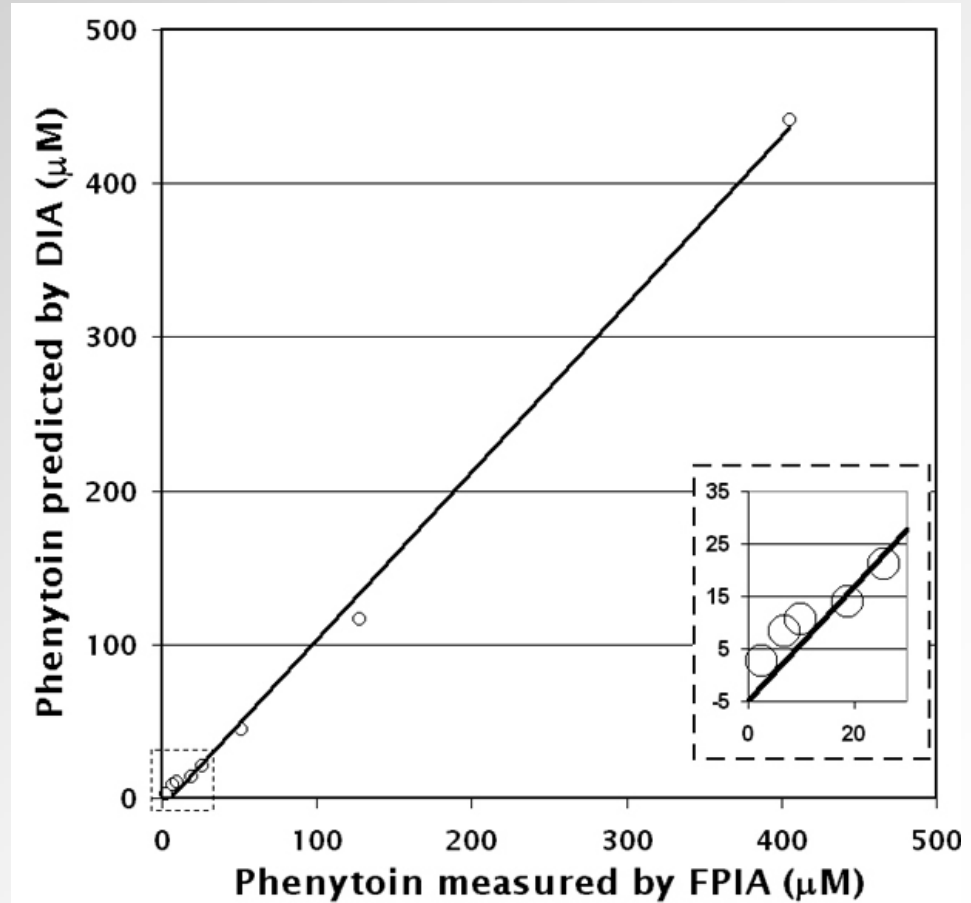
- **Modeling:** a 1D simulation of the phenytoin experiment
- Model has been used to design improved devices and optimize reagent concentrations





# DIA compared to FPIA

- DIA tests of blood samples compared to FPIA measurements.
- DIA compared favorably with FPIA for wide range of sample concentrations.
- The open circles were NOT used to form the calibration line





# NCRR DIA Project Status

- Implemented successful immunoassay in a T-Sensor for detecting a small analytes.
- Implemented successful immunoassay in hydrogels in a 96-well format for detecting small analytes.
- Demonstrated measurement of phenytoin concentrations from 1 nM to 1  $\mu$ M *in less than 30 seconds* in diluted whole blood.
- Currently demonstrating detection of larger molecules.



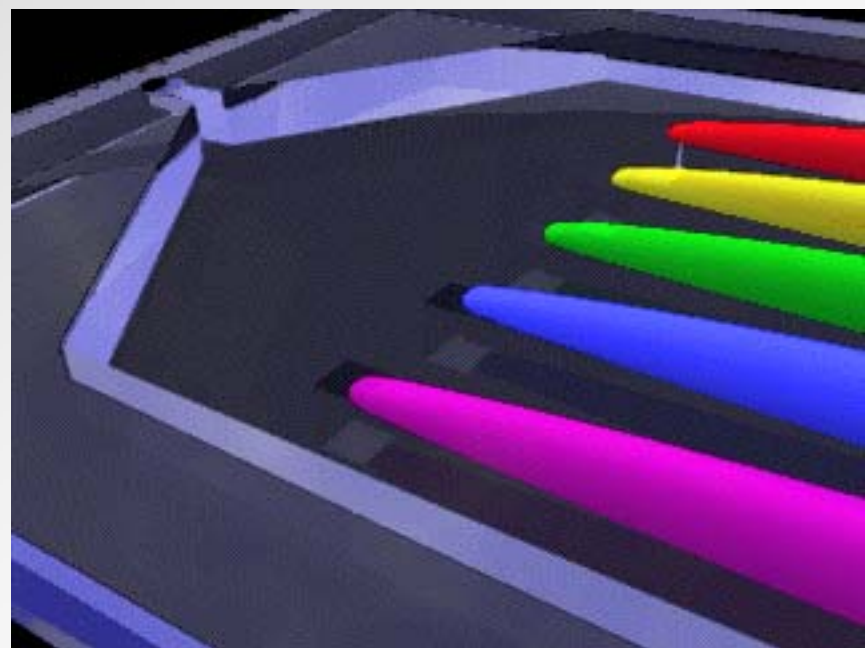
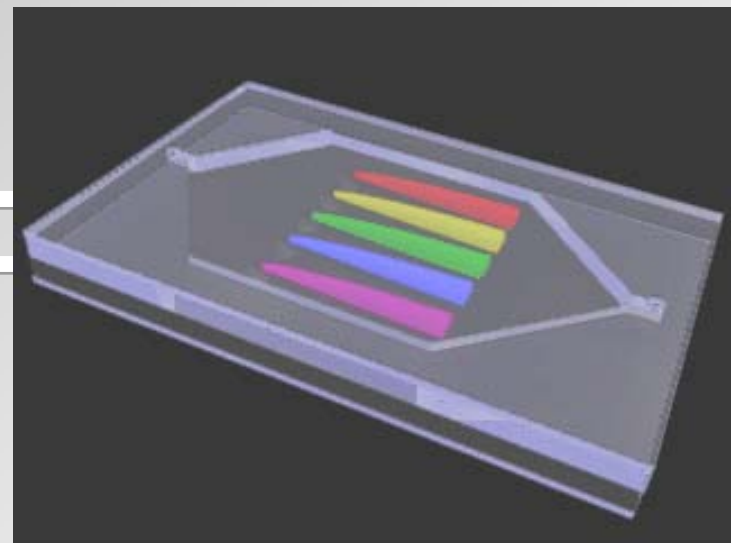
# DIA Challenges

- How to multiplex the DIA and related assays without filling a room with syringe pumps?
- How to preserve reagents on the laminate until time of use?



# Multiplexing the T-Sensor in a Polymeric Laminate

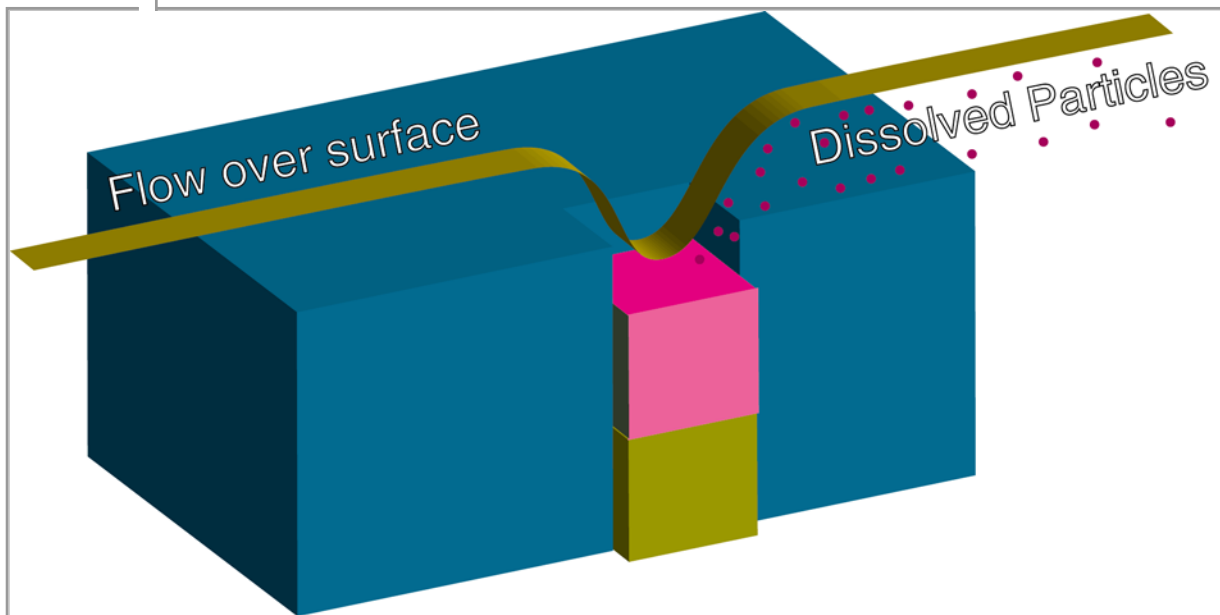
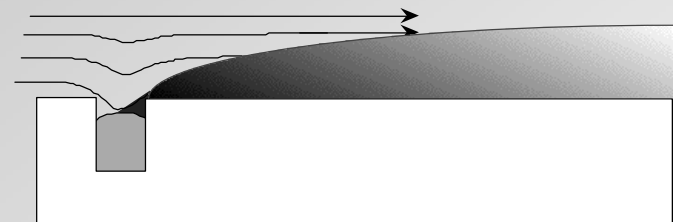
- The “Flat T-sensor” concept is the use of multiple interdiffusing streams.
- Molecular binding and other interactions can be detected at the points of overlap between the streams and the analyte.
- The device is “started” by wetting out.
- *This approach greatly simplifies the fluid controls required!*







# Dry Reagent Delivery



How to create controlled streams of multiple reagents without multiple pumps?  
Blocks of one or more materials dissolve as the fluid flows over them.

- We have begun to explore the use of dissolution of dry plugs of material to produce interdiffusing streams.
- Flow over dry reagents will cause controlled dissolution of the reagents, creating “plumes” of reagents downstream
- These plumes can either be used for reaction in solution, or for creating patterned capture surfaces downstream





# Dissolution of sample in cavity in PDMS

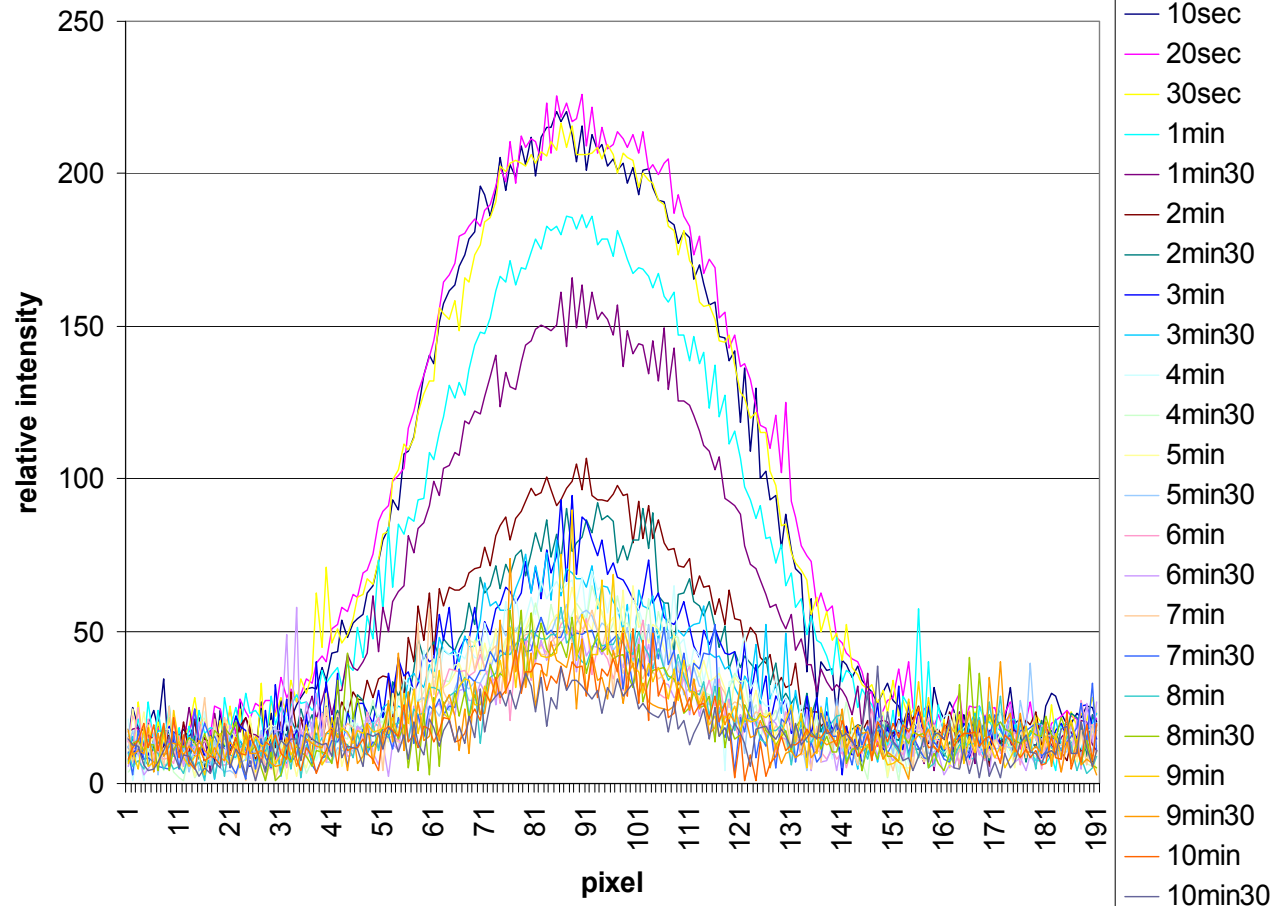
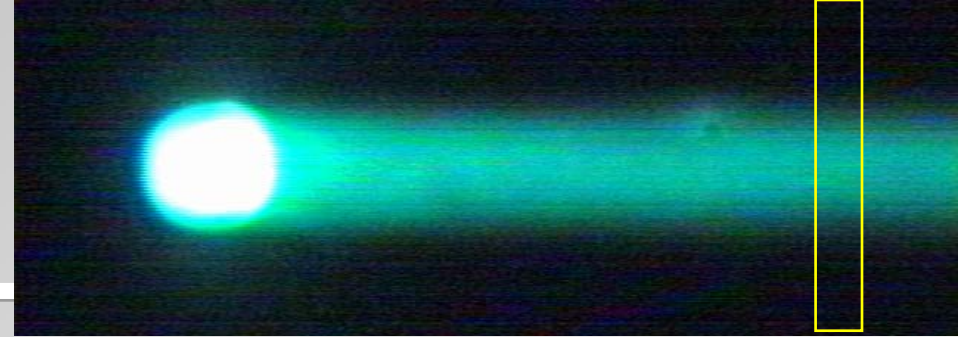
- 200  $\mu\text{m}$  x 200 $\mu\text{m}$  cylindrical hole in PDMS
- Filled with dry trehalose-dextran matrix and fluorescein as a label
- Dissolution measurable for >10 minutes
- Dissolution controllable by fraction of dextran
- After wet-out, shape of plume appears constant even though overall intensity drops.

QuickTime™ and a DV - NTSC decompressor are needed to see this picture.

*Flow from left to right. Movie begins just after arrival of the solvent front*



# Plume stability



- Note that plume intensity drops to 50% by ~2 min.
- Further control possible by shape and depth of hole, dextran concentration, diffusivity of solute, flow rate, etc.



# Modeling Dissolution

QuickTime™ and a YUV420 codec decompressor are needed to see this picture.

- Modeling is ongoing in collaboration with Bruce Finlayson of ChemE
- Shown--a 2D CFD model (FEMlab) of dissolution of low viscosity reagent in cavity in channel.



# Optimizing the Modeling

QuickTime™ and a YUV420 codec decompressor are needed to see this picture.

- The solution in the cavity is now 11 times more concentrated in solute, which increase the viscosity 11 times.
- The viscosity changes as the solute concentration drops.



# Limits to the DIA

- The DIA and all other T-sensor embodiments are “homogeneous assays” in which all the chemistry (hopefully) occurs in the solution phase.
- To date the minimum analyte concentration measured with the DIA is about 0.3 nM.
- Many analytes of interest in biological systems are present at much lower concentrations
- *To measure these, some form of solid phase must be employed to capture the analyte to allow it to accumulate prior to measurement.*

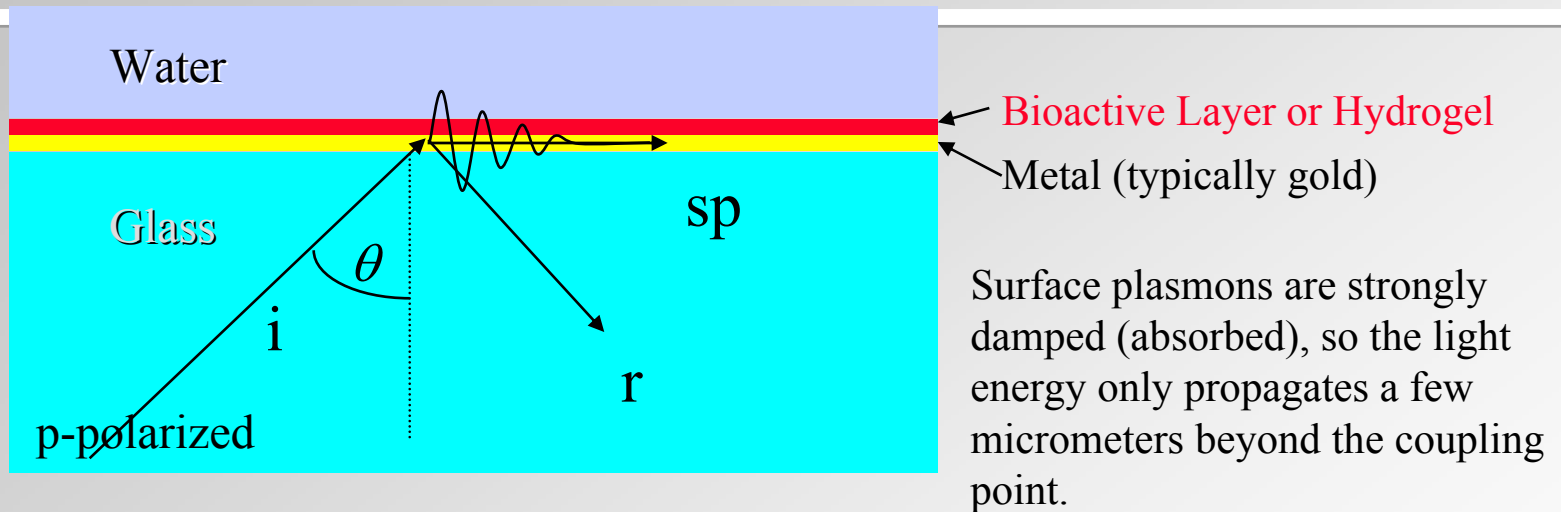


# Surface Plasmon Resonance (SPR)

- No labeling required of reagents
- Accumulation of things on walls for sensitivity
- Generic detection of anything--small molecules large molecules, beads or pathogens
- Basic principles well known
- Commercial products already available (e.g., Biacore and TI's SPREETA)
- Inherently inexpensive
- Easily coupled to microfluidics
- Amenable to multiplexing for many samples



# Surface Plasmon Resonance Operating Principle (after Kretschmann)



For a given metal film thickness, light at one frequency will, at a particular angle  $\theta$ , resonate with plasmons in the metal film.

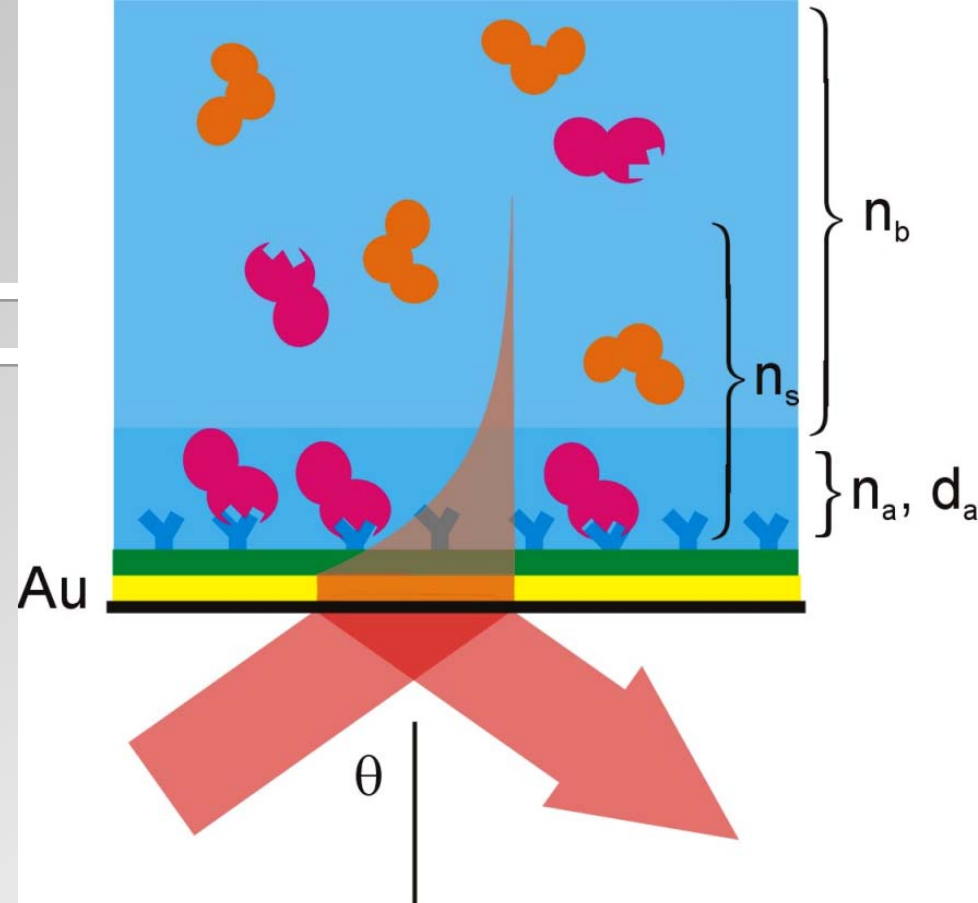
The resonance greatly reduces the reflectivity.

The refractive index *in the plasmon field* on the far side of the film strongly influences the conditions for resonance



# Real SPR

- Schematic representation (not to scale) of detection of surface binding events using SPR.
- Capture molecules are attached to the surface of the film that overlies the gold film.
- The capture layer may be a monolayer or a thick layer as in the dextran films sold by Biacore for use in their instrument.
- The field that senses the refractive index ( $n$ ) penetrates a large fraction of  $1 \mu\text{m}$ .
- It therefore senses both the refractive index of the surface film  $n_a$ , but *also the refractive index of the solution beyond that surface film* out to the point where the field strength drops to zero.



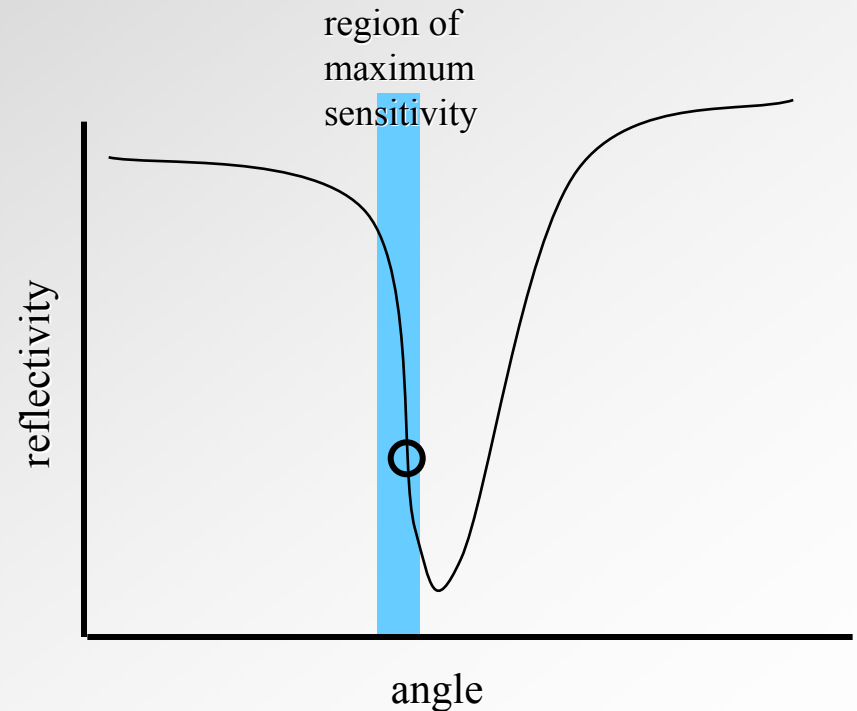
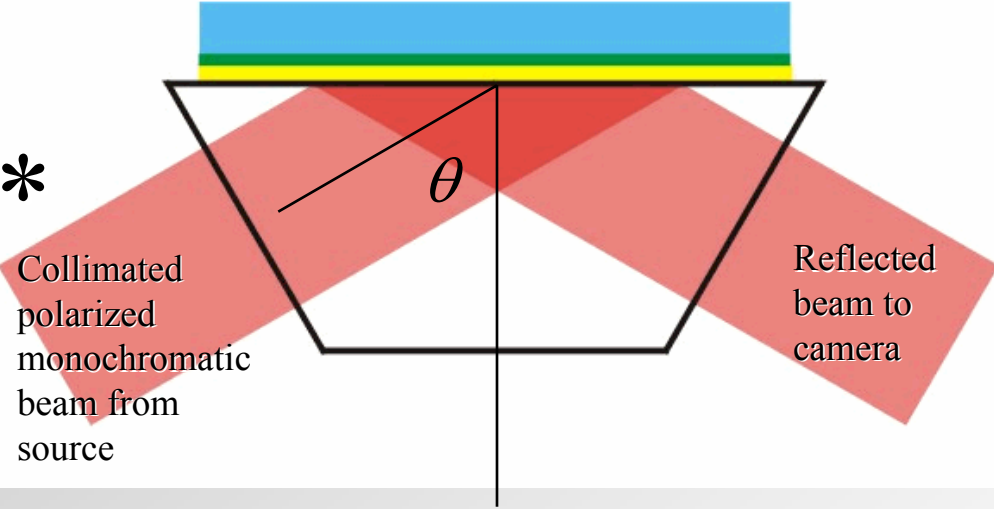




# SPR Imaging\*

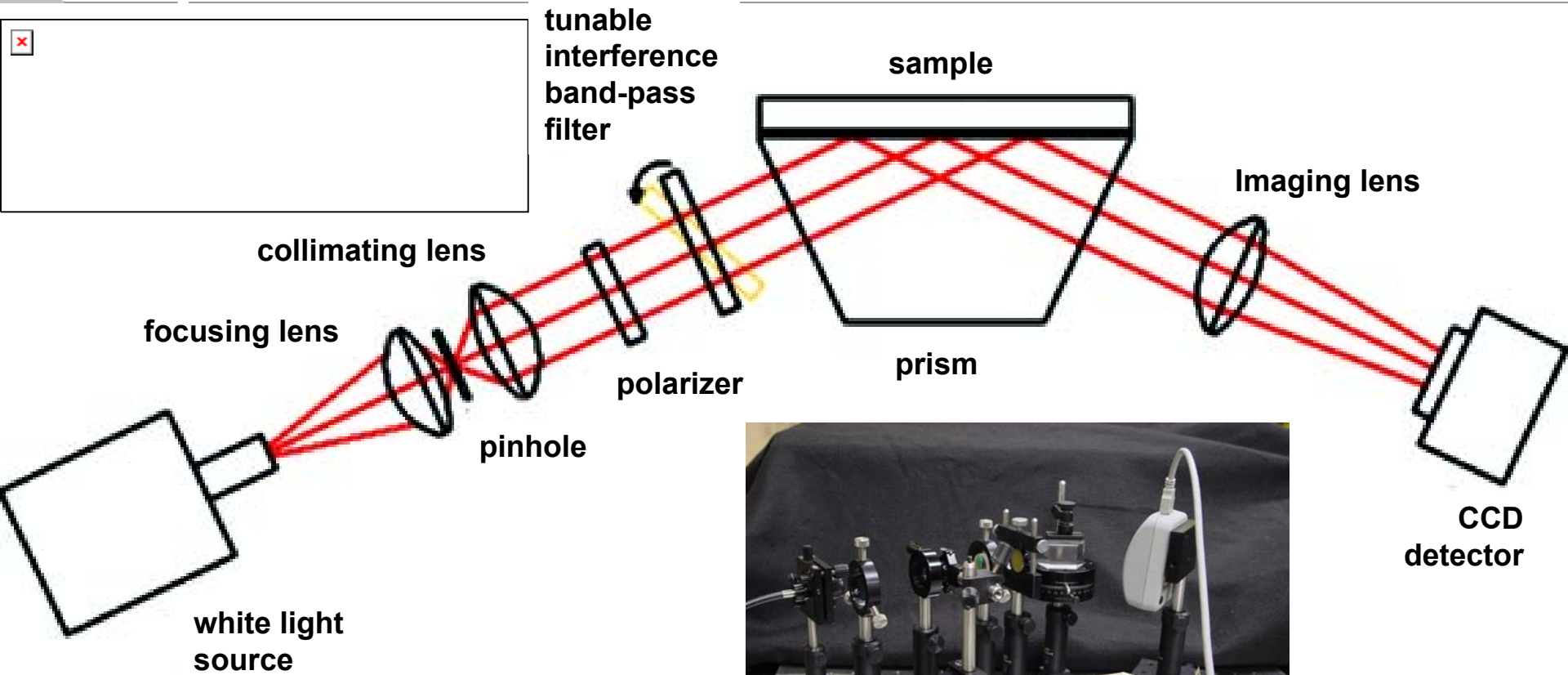
- On the assumption that analytes will increase the refractive index  $n$  of the sample, poise the angle  $\theta$  at the point where any change in  $n$  produces the largest change in reflectivity
- Changes in  $n$  produce features whose intensity can be correlated with concentration of material at or near the surface

\*the newest SPR technique





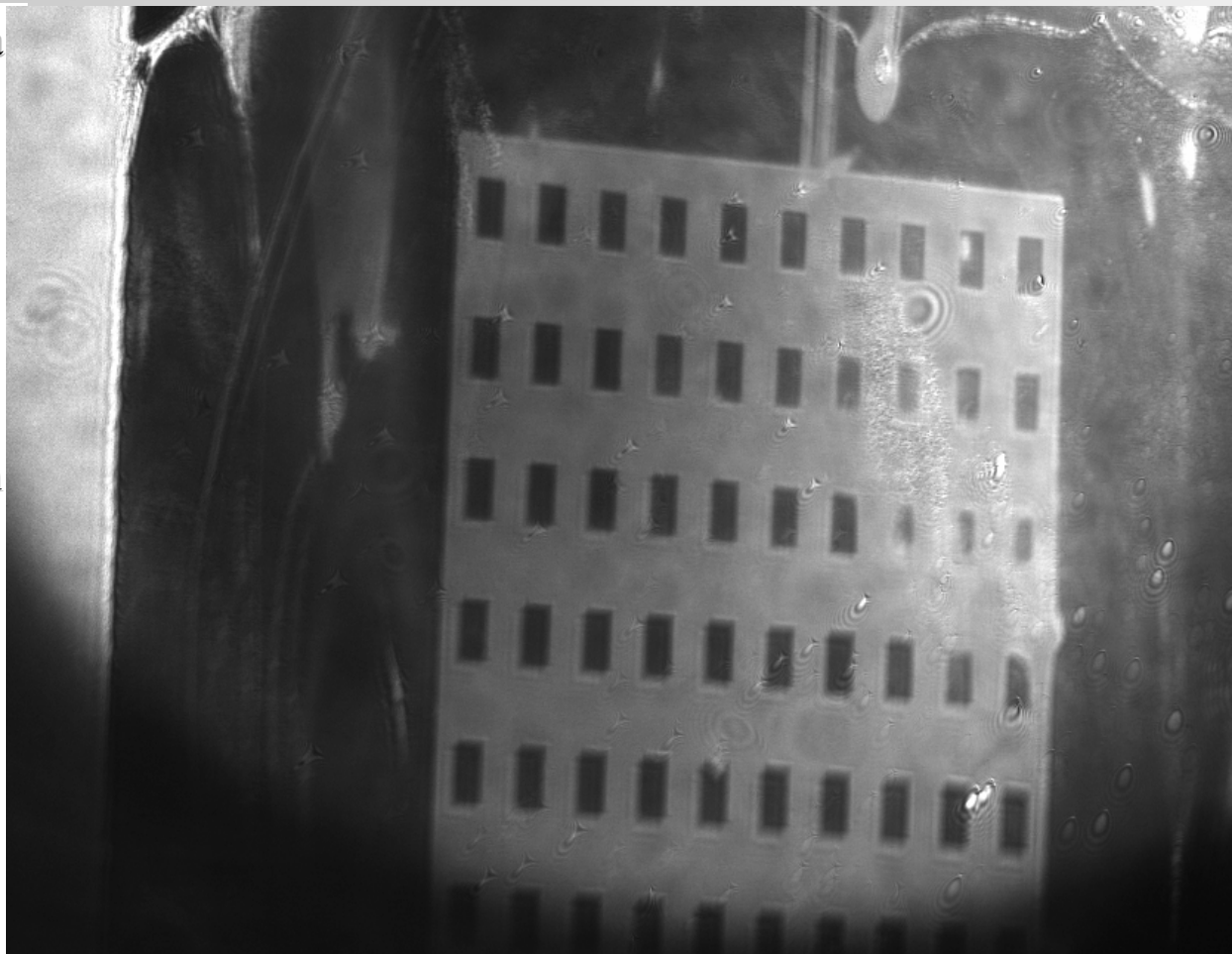
# Design of Yager Lab SPR Microscope





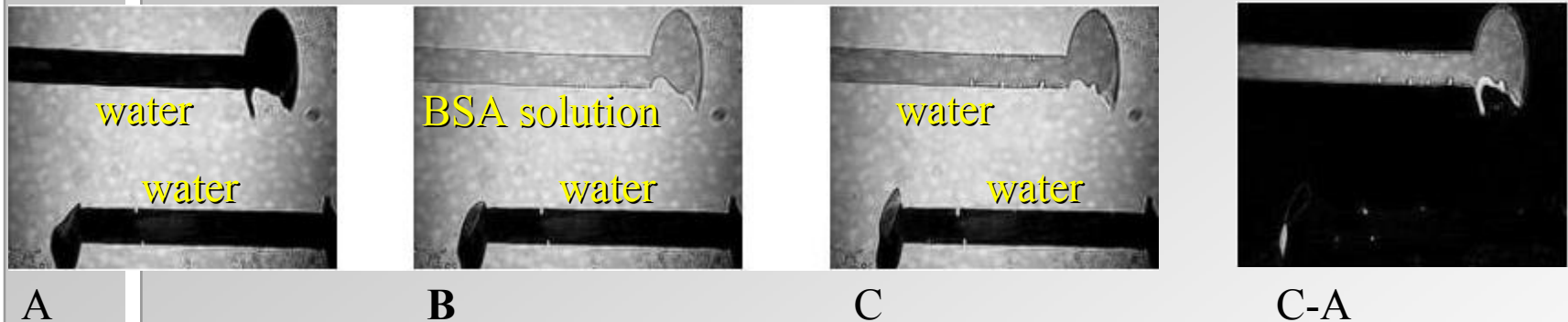
# Recent SPR Microscope Images

- An SPR image taken with a B&W CCD camera.
- The pattern was made by stamping  $C_{16}$  alkane thiols onto the gold surface to produce one monolayer.
- The gold surface was then covered by a laminate-based fluid chamber, which was filled with buffer before imaging
- The stamp surface contained  $500\mu\text{m} \times 500\mu\text{m}$  pits that produced the dark rectangles in the image. The rectangular shape is due to the foreshortening of the image.





# Protein Film Detection by SPR Microscopy

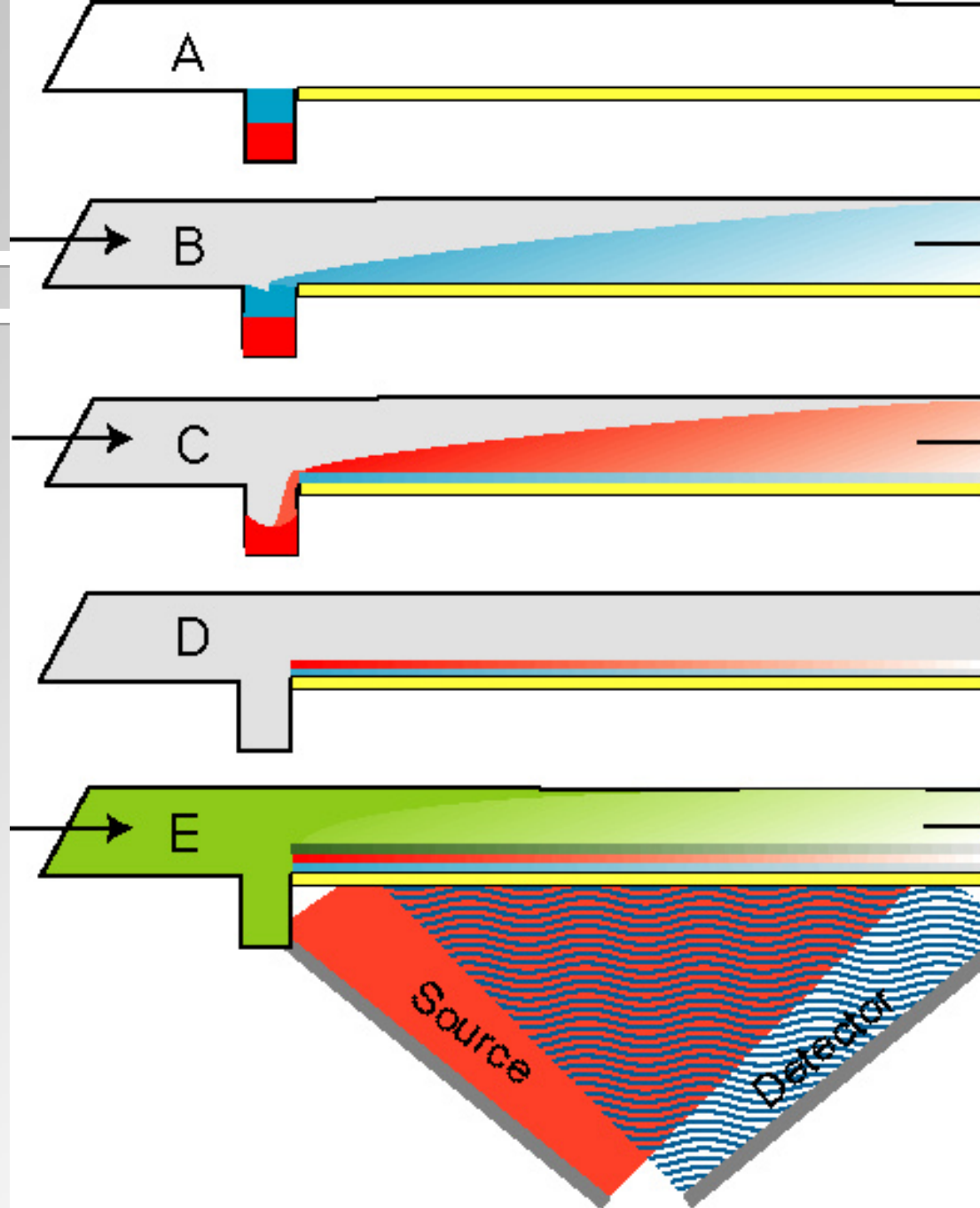


- Detection of adsorption of a monolayer of the protein bovine serum albumin (BSA) onto the Au surface
- In B a  $\sim 2$  mg/ml solution of BSA in PBS flows through
- In C is the channel after extensive rinsing with water
- C-A shows the presence of the film in the upper channel, and no change (except the formation of a few bubbles) in the lower channel



# SPR Sensor Concept

- A) Antibodies (blue) are stored dry and stable in a well in the wall of a microchannel in a single-use device.
- B) When the device is wetted-out antibodies dissolve, flow downstream, diffuse to and coat the gold surface,
- C) The antibody coating varies in density depending on position,
- D) Analyte-laden sample flows over the now-activated gold surface.
- E) SPR optical probing of the position-dependent refractive index of the coated surface is made from below with "permanent" inexpensive optical components.

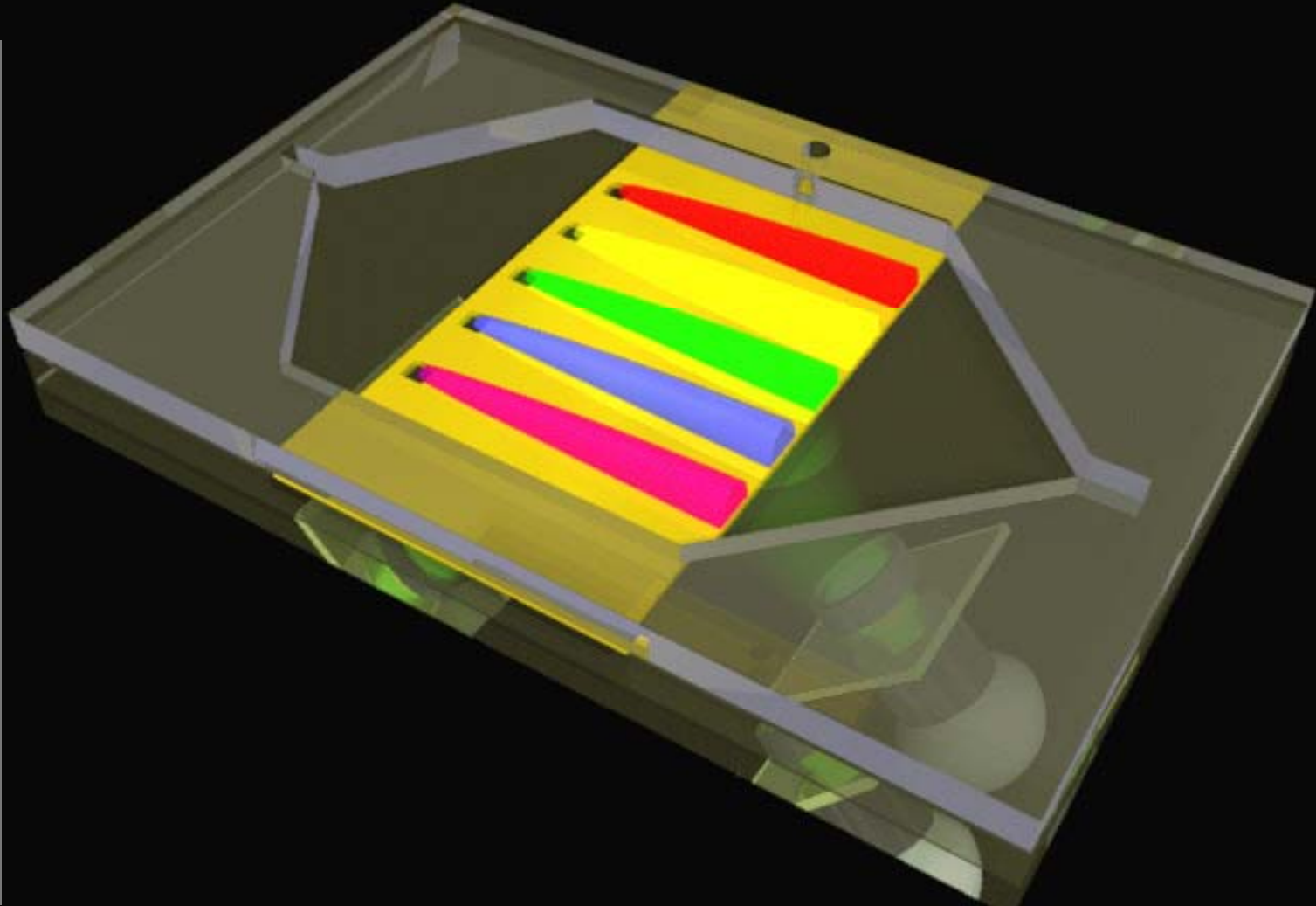






# An inexpensive SPR-based disposable

- Reagents would be stored dry and rehydrated during wet-out
- Placing 20 channels in a 1 cm square is feasible.
- The gold surface on the laminate would be accessible from below for SPR and from above for fluorescence imaging





# Yager Lab Ongoing Projects

- Development of diffusion immunoassay (DIA) to detect clinically-relevant analytes in whole blood
- Creation of systems for multiple parallel point-of-care immunoassays in an inexpensive disposable
- Surface plasmon resonance microscopy for POC diagnostics
- Controlled mixing of solutions that combine to form aggregates
- Rapid extraction of DNA from whole bacteria
- Development of systems for analysis of saliva



# Acknowledgements

- Many collaborators, post-docs and both graduate and undergraduate students (see www site)
- The Washington Technology Center (1993-present)
- DARPA Defense Sciences Office (1994-1996)
- Senmed Medical Ventures / Micronics, Inc. (1994-present)\*
- DARPA MEMS/MicroFlumes Program (1997-2000)
- MesoSystems, Inc. (2000-present)
- NIH NCRR (2001-present)
- Amgen Corporation (2002-present)
- NIH NIDCR (2002-present)
- Singapore's A\*STAR (2002-present)
- \* Yager has a financial interest in Micronics



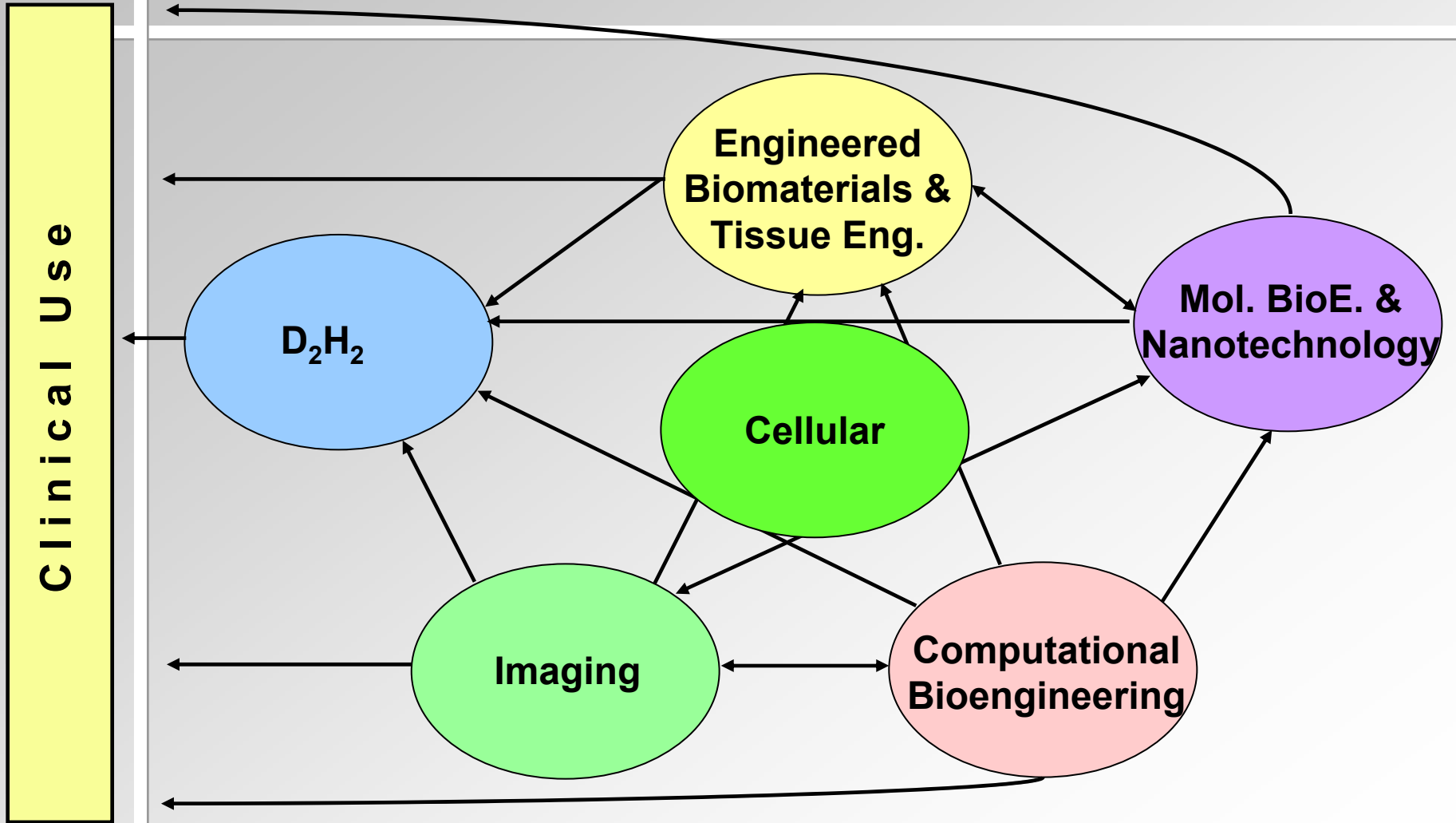




Fin



# UW BioE Research Thrust Areas





# Accounting for Molecular Interactions with Surfaces in Flow

